

# Multiscale structure-functional modeling of musculoskeletal mineralized tissues

Ra 1380/7-1

K. Raum<sup>1</sup> and A. Gerisch<sup>2</sup>

Ge 1894/3-1

<sup>1</sup>Q-BAM Group, Dept. of Orthopedics, Martin Luther University of Halle-Wittenberg, Germany<sup>2</sup>Institute of Mathematics, Martin Luther University of Halle-Wittenberg, Germany

## Summary

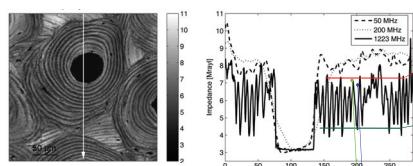
Musculoskeletal mineralized tissues (MMTs) achieve a unique combination & variability of stiffness and strength with one common building block & structural hierarchy.

### Material properties + hierarchical structure = macroscopic elastic function

Hypothesis: multiscale experimental elastic data & numerical homogenization allow to decouple structural & material properties and their respective impacts on the elastic functional behavior of the compound.

## Nanoscale - mineralized collagen fibril

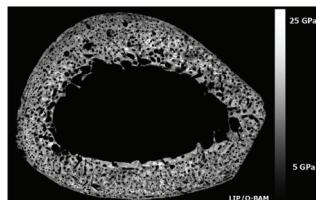
- well known structure and elastic properties of major components (hydroxyapatite, collagen, water)
- variable mineral deposition & platelet size
- self assembly mechanisms lead to dense regular structures [1]



- 1 - 1.5 GHz SAM [5] lamellar unit size & transverse isotropic stiffness of fibril bundles
- Nanoindentation** (small indentation depth) [6] Goal: anisotropic elastic modulus & Poisson ratios

## Microscale

- 50 - 200 MHz SAM [7] heterogeneous tissue elasticity & porous microstructure
- Nanoindentation** (large indentation depth) [6] Goal: anisotropic elastic modulus & Poisson ratios



## Mesoscale / Macroscale

- Low frequency ultrasound (1 - 10 mm) orthotropic tissue elasticity
- Mechanical testing** (> 5 mm) anisotropic elastic modulus

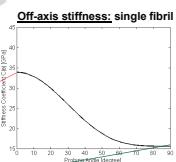


## Numerical "Bottom-Up" Model

### M-I Mineralized Fibril

Goal: time-dependent intra- & interfibrillar mineral deposition and mineral growth[2]

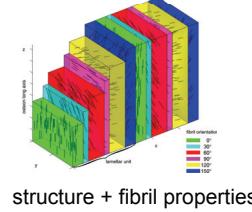
$$\text{transverse isotropic stiffness tensor } C_{\text{eff}}^{\text{nano}} = f(t)$$



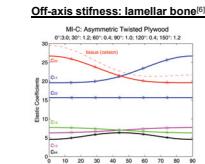
Comparison with exp. data

$C_{ij}$ [GPa]	SAM [3]	NI [4]
$C_{33}$	33.9	40.6
$C_{11}$	15.6	32.8
$C_{12}$	5.2	15.1
$C_{32}$	8.8	17.5
$C_{44}$	3.4	9.1

### M-II Lamellar Bone [3]



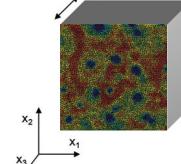
$$C_{\text{eff}}^{\text{micro}} = f(C_{\text{exp}}^{\text{nano}}(\vec{x}))$$



structure + fibril properties

orthotropic stiffness tensor

### M-III Mesoscale Model [7]



$$C_{\text{eff}}^{\text{meso}} = f(C_{\text{exp}}^{\text{micro}}(\vec{x}))$$

porous structure + heterogeneous tissue properties at 1-mm length scale

orthotropic stiffness tensor

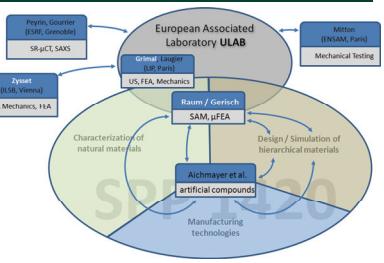
## Macroscale Simulation



Goal:  
suitable & realistic  
input for standard FE  
analysis

## Outcomes

- Linked experimental assessment / numerical modeling of mechanical function of MMTs at several length scales.
- Validation of the results by cross-validation at all scales.
- Tool to simulate mechanical outcome of compositional /structural alterations (e.g. maturation, pathologies)
- Application to biomimetic hierarchically structured materials (Aichmayer).



**Principal International Collaboration Partners:**  
Q. Grimal, Laboratoire d'Imagerie Paramétrique, CNRS, Paris  
P. Zytnet, Institut f. Leichtbau und Struktur-Biomechanik, Wien  
ULAB: Ultrasound bases Assessment of Bone

## Homogenization

**Input** inhomogeneous material tensor  $C(\vec{x})$  with small scale variations in Representative Volume Element (RVE).

**Objective** find effective material tensor  $C_{\text{eff}}$  for RVE, such that mechanical responses of RVE with  $C(\vec{x})$  and  $C_{\text{eff}}$  are similar.

**Method** Numerical homogenization, i.e. compute  $C_{\text{eff}}$  from spatially averaged results of the solution of the equations of linear elasticity in the RVE subjected to specific loading conditions and using  $C(\vec{x})$ .

**Implementation** Finite Element Method (FEM) using Comsol Multiphysics and high resolution experimentally derived elastic input data.

**Application** use  $C_{\text{eff}}$  as input for the FE simulations on larger scales.

**Mathematical challenges** choice of loading conditions; accuracy control and speed-up of the FE solution; sensitivity investigations.

## Samples

Tissue type	Origin	Mineral content	Fiber Orientation	Periodic Size
Mineralized tendon	Turkey	< 50 wt%	parallel	up to 1 mm
Parallel-fibered bone	Young cattle	~ 65 wt%	parallel	~ 100 μm
Plexiform bone	Cattle		parallel + lamellar	~ 100 μm
Plywood structure	Mature cattle, Human	30-70 wt%	orthogonal twisted (osteons, interstitial tissue)	< 5 μm
Artificial compound	MPI Golm Aichmayer	n.a.	parallel	< 1 cm

## Definition of Length Scales

Length scale	Composition	Compound	Nomenclature
1 - 200 nm	hydroxyapatite, collagen, water, other	mineralized collagen fibril	nanoscale
0.2 - 10 μm	mineralized collagen fibrils, pores	mineralized tissue matrix (variable structures)	microscale
0.01 - 1 mm	mineralized tissue matrix, pores	MMTs	mesoscale
> 1 mm	MMTs, macrostructure	organs	macroscale

## References

- [1] Giraud-Guille et al. J Biomech, 2006
- [2] Ruffoni et al. Bone, 2008
- [3] Raum et al. IEEE US-Symp, 2007
- [4] Hofmann et al. J Biomech, 2006
- [5] Raum IEEE UFCC, 2008
- [6] Franzoso et al. J Biomech Eng, 2008
- [7] Raum et al. Phys Med Biol, 2006
- [8] Grimal et al. Comput Meth Biomed Eng, 2008